

Mastering MRI Designs through Component Selection

Mark van Uden Tesla Dynamic Coils 05-02-2024



MEDISCHE ELEKTRONICA Ontwikkelingen, normen en toepassingen



Tesla Dynamic Coils

- Work for about 20 years in the field of MR scanners
 - Philips Healthcare
 - RadboudUMC
 - Tesla Dynamic Coils
- Based in Zaltbommel
- We develop and built RF coils, peripheral electronics, cables, mechanical for MRI scanners
- ISO 13485:2016 certified





Topics

- Nuclear magnetic resonance
- Scanner
- RF coils
- Components and designs
 - Static magnetic field distortion
 - Transmit (receive) coils
 - Receive coils
 - Testing





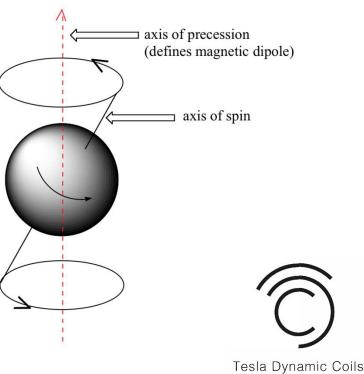




Nuclear magnetic resonance

- Frequency is determined by:
 - Magnetic field strength
 - Gyromagnetic ratio
 - Nuclei: ¹H, ³¹P, ¹³C, ...
 - Ranges between 30 MHz and 300 MHz
- MRI: Magnetic Resonance Imaging medical application



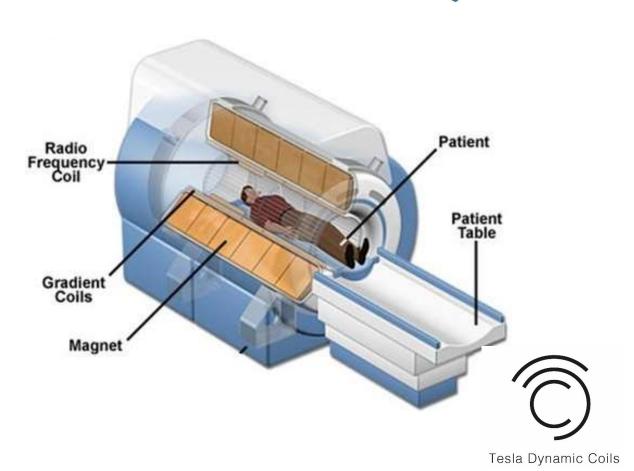




Sponsored by:

MR Scanner

- Magnet
- RF coils
- Gradient coils
- Patient table
- Patient





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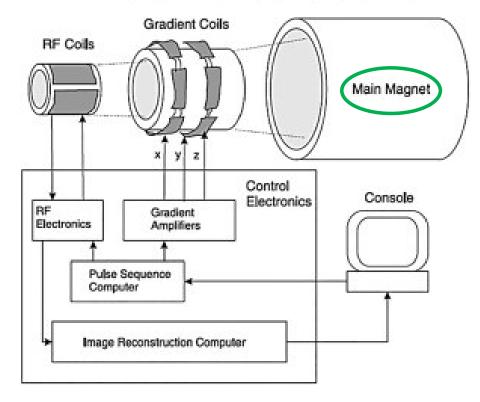




MR Scanner

- Magnet (B0)
 - 0 Hz
 - 3 7 Tesla
- RF coils (B1+)
 - 30 300 MHz
 - Max. 50 μT
 - Max. 35 kW peak
 - Max. 250W average
- Gradient coils
 - 1 5kHz
 - 200 mT/m
 - 200 T/m/s

MRI Scanner Components





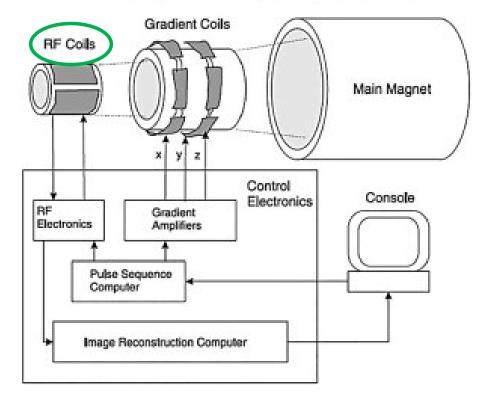




MR Scanner

- Magnet (B0)
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MRI Scanner Components





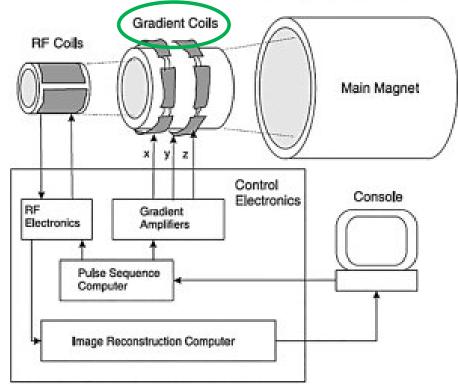


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MRI Scanner Components







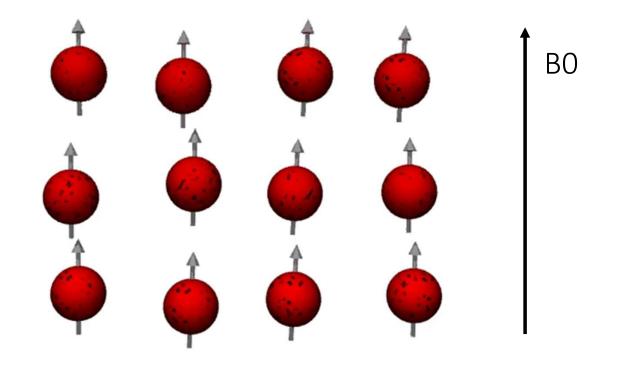


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Nuclear magnetic resonance

■ Transmit and/or receive on frequency of interest

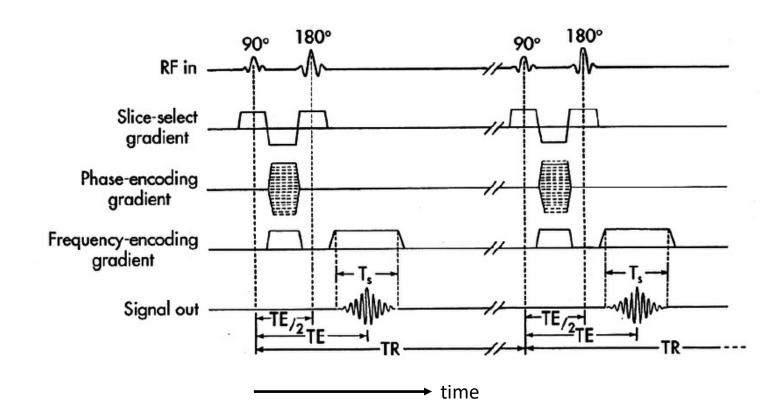


https://www.youtube.com/watch?v=0YBU
SOrH0Iw



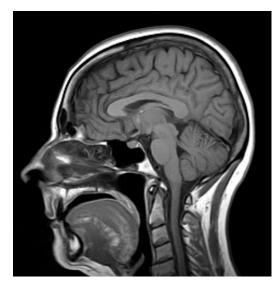
MR Scanner

- Combine RF pulses and gradient fields
- Right timing
- Image/spectrum

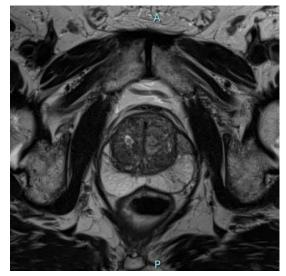


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MR Scanner



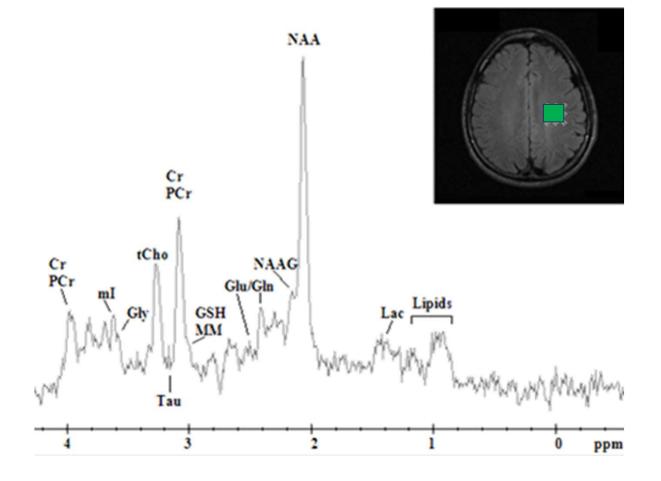








MR Scanner





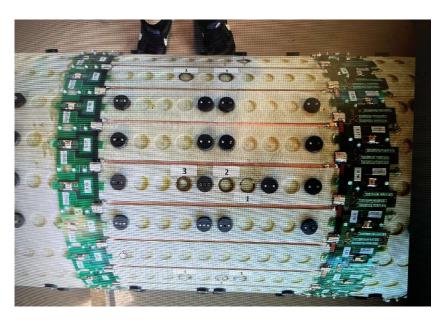




Sponsored by: hcyncn

RF coils







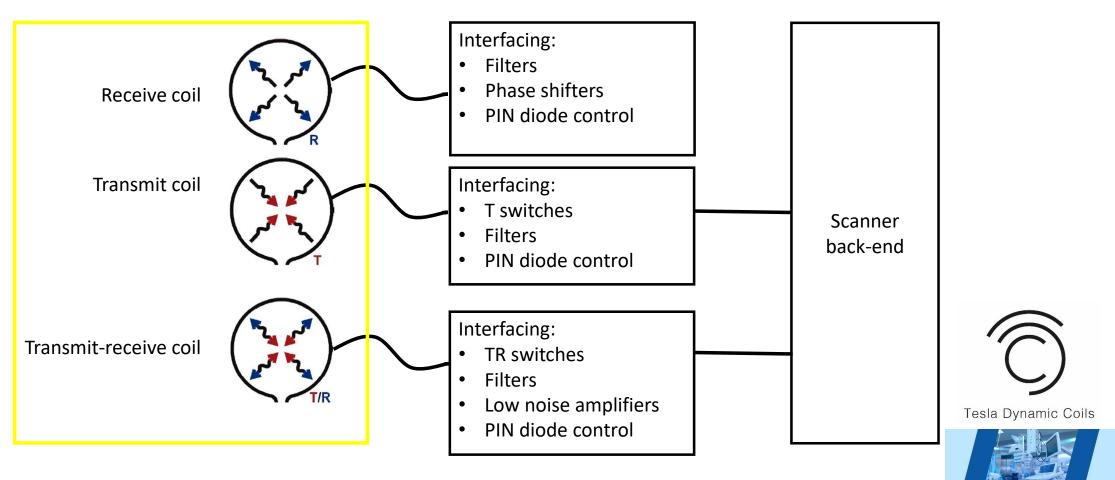




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RF coils



Components and designs

- Capacitors
- Inductors
 - RF
 - DC/chokes
 - Traces
- Resistors
- Low Noise Amplifiers
- Fuses

- Diodes
 - PIN diodes
 - Fast diodes
 - ESD suppression
- RF connectors
 - BNC
 - SMA
 - SMB
 - N



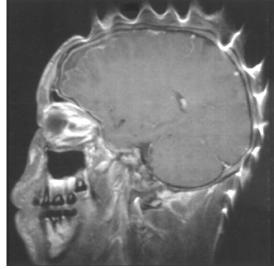






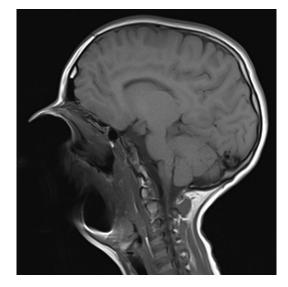
Distortion of main magnetic field in imaging Field Of View (FOV)

Hair gel



https://www.ajronline.org/doi/10.2214/ajr.182.2.1820532

Braces



https://mriquestions.com/susceptibility-artifact.html







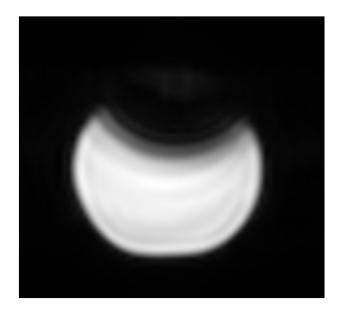
Test protocol on MR scanner







N connector





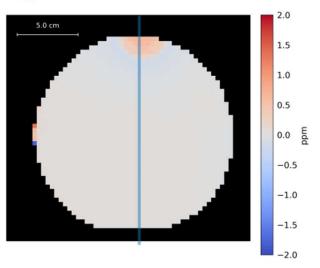




Test protocol on MR scanner

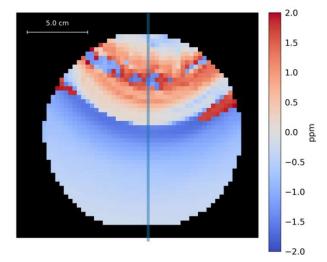
M4 screw

Half ppm distance: 7 mm



N connector

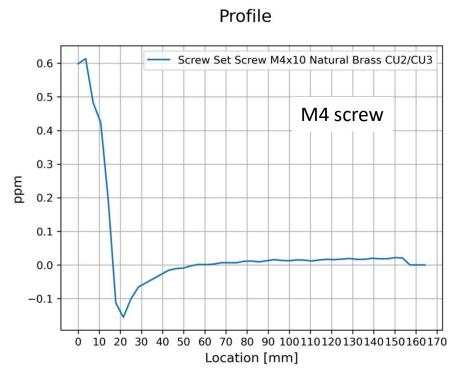
Half ppm distance: 126 mm

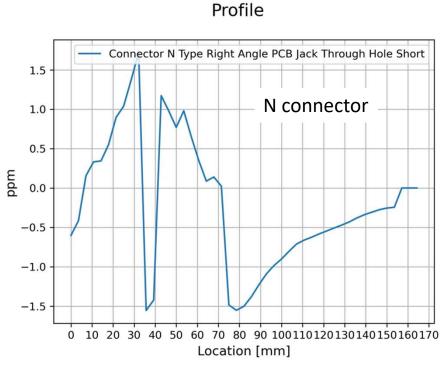






Test protocol on MR scanner



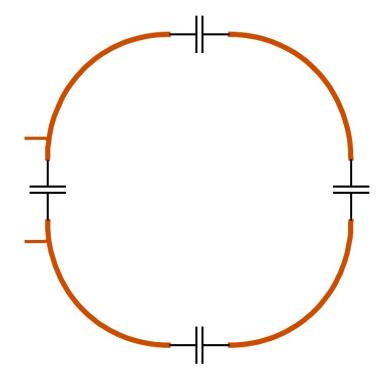






- Loading of RF coil
- EM fields couples to conducting substance



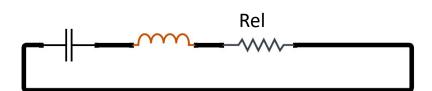


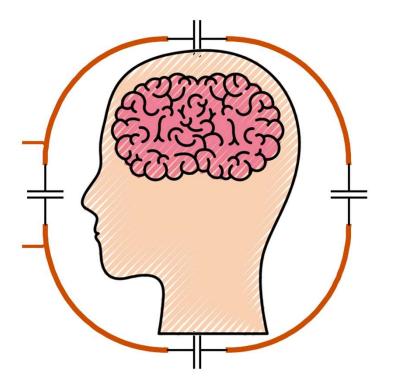






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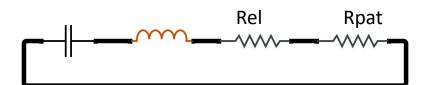


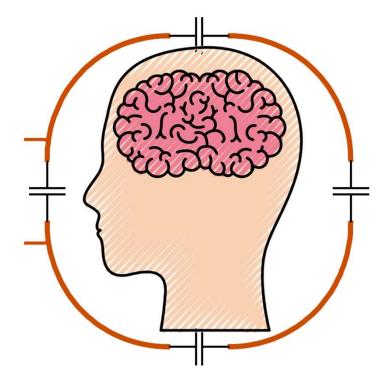






- Loading of RF coil
- EM fields couples to conducting substance
- Quality factor drops



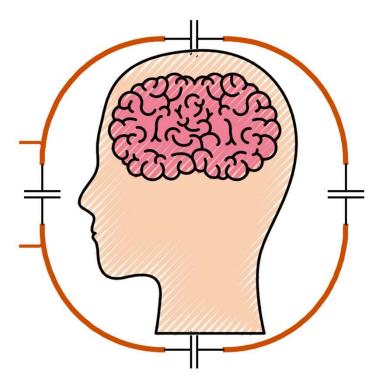








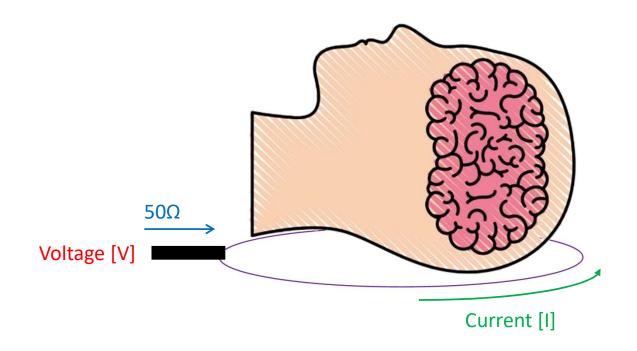
- Specific absorption rate (SAR)
- E-field
- Great effort put in prediction







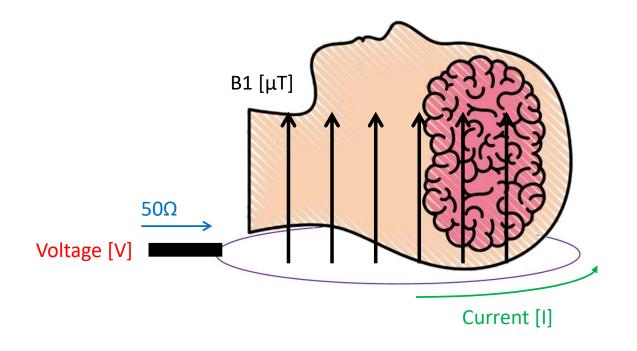










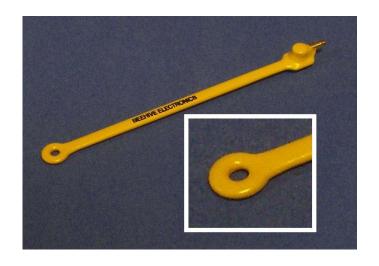








- How much B1+/V is generated by a coil
 - Measure pick up probe

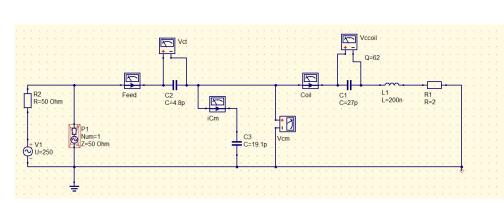


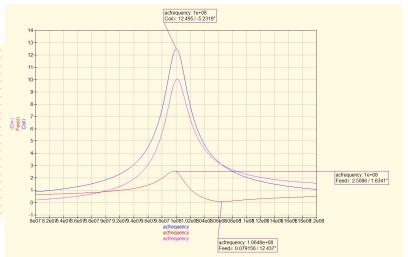






- How much B1+/V is generated by a coil
 - Measure pick up probe
 - Circuit simulation





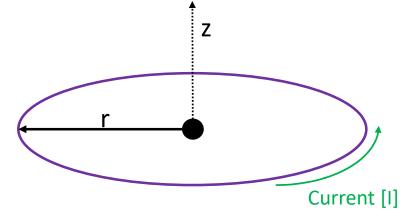






- How much B1+/V is generated by a coil
 - Measure pick up probe
 - Circuit simulation
- Tissue does change the EM field

$$B_Z = \frac{\mu_0}{4\pi} * \frac{2\pi r^2 I}{(z^2 + r^2)^{3/2}}$$

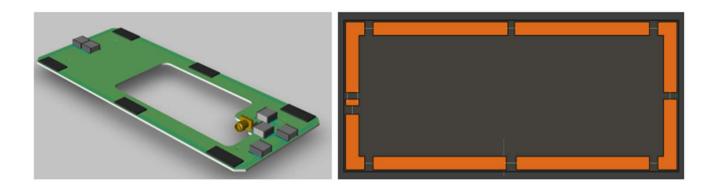








- How much B1+/V is generated by a coil
 - Measure pick up probe
 - Circuit simulation
 - EM field simulation

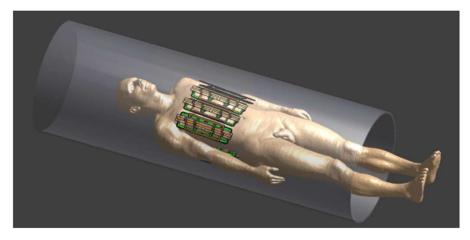


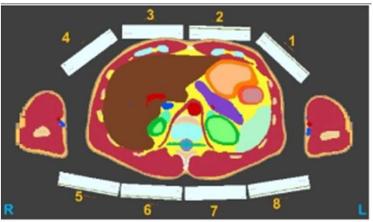






- How much B1+/V is generated by a coil
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 - Circuit simulation
 - EM field simulation

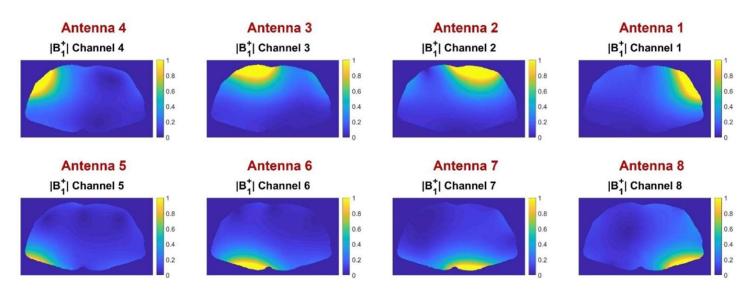








- How much B1+/V is generated by a coil
 - Measure pick up probe
 - Circuit simulation
 - EM field simulation







- How much B1+/V is generated by a coil
 - Measure pick up probe
 - Circuit simulation
 - EM field simulation
 - Measure on MR scanner
 - B1+ map
 - Flip angle train







- Scale voltage and currents to desired B1+ field
- Or maximum output of the RF power amplifier of the scanner
- Compare scaled values to datasheet







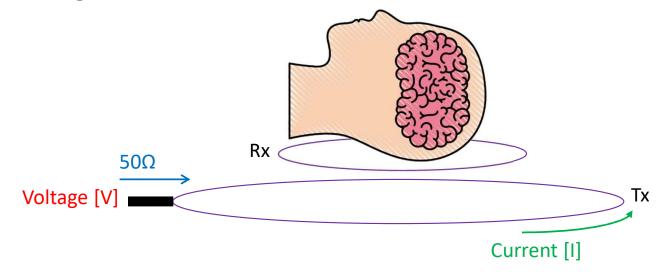
- Pick up the tiny RF signals
- Positioned close to the patient
- Losses (resistance) result in lower SNR
- Rx coils must be combined with a Tx coil
- They are exposed to high B1 fields







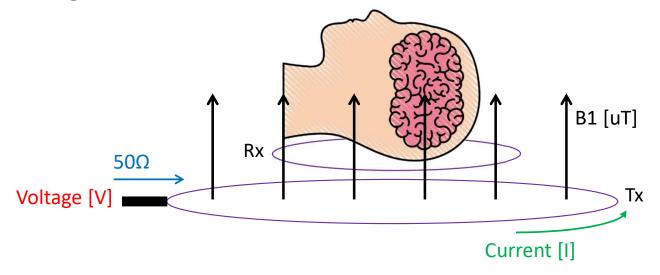
- During transmit voltage induced
- Induced voltage creates a current
- Current generates own magnetic field
- Disturb original B1 field







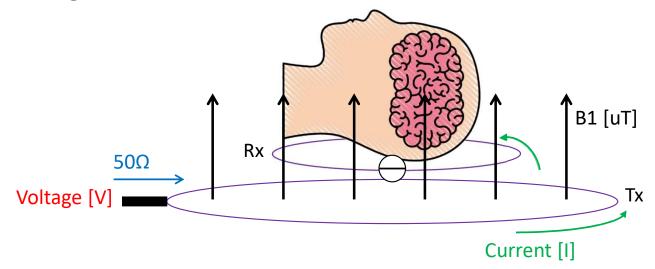
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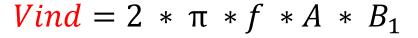






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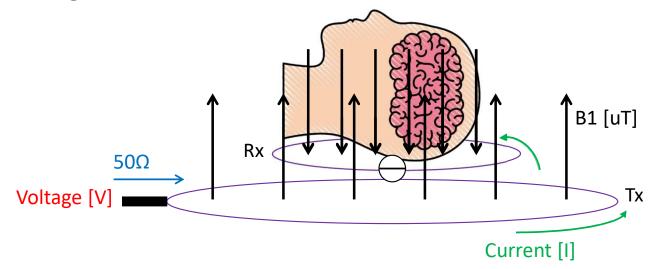


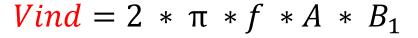






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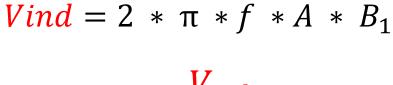




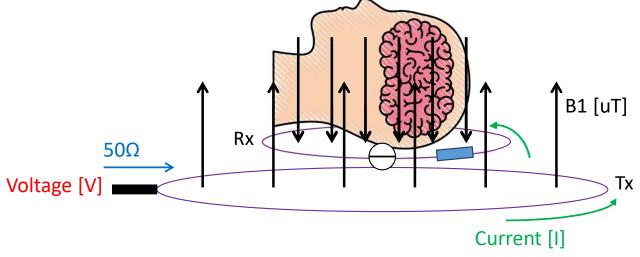




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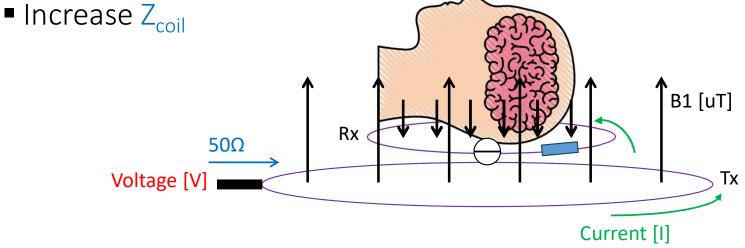
$$I_{coil} = \frac{V_{ind}}{Z_{coil}}$$







- During transmit voltage induced
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$$Vind = 2 * \pi * f * A * B_1$$

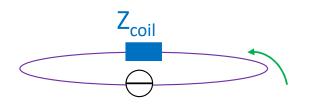
$$I_{coil} = \frac{V_{ind}}{Z_{coil}}$$

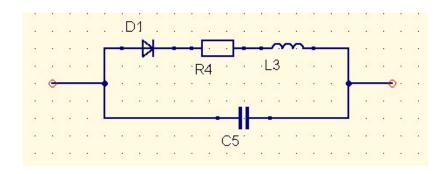






- High Zcoil means low SNR
- Switch the high impedance on and off: detune circuits
- PIN diode biasing



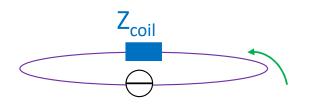


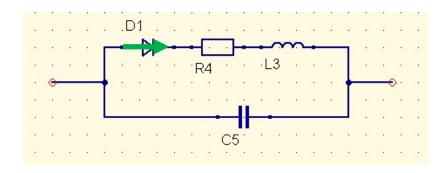






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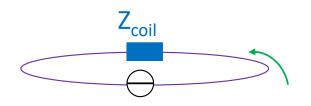


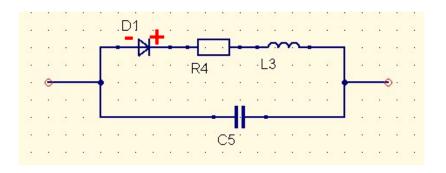






- High Zcoil means low SNR
- Switch the high impedance on and off: detune circuits
- PIN diode biasing











- Missing specifications
- Experience and common practice
- +60dBm CW ≠ 8kW puls

Absolute Maximum Ratings¹ @ 25°C

Parameter	Absolute Maximum
Operating Temperature	-65°C to +125°C
Storage Temperature	-65°C to +150°C
Diode Junction Temperature	+175°C Continuous
Diode Mounting Temperature	+265°C for 10 seconds
RF C.W. Incident Power	+ 60 dBm C.W.
Forward D.C. Current	+500mA
Reverse D.C. Voltage @ -10µA	-1100V

 Exceeding these limits may cause permanent damage.







Components and designs: Testing



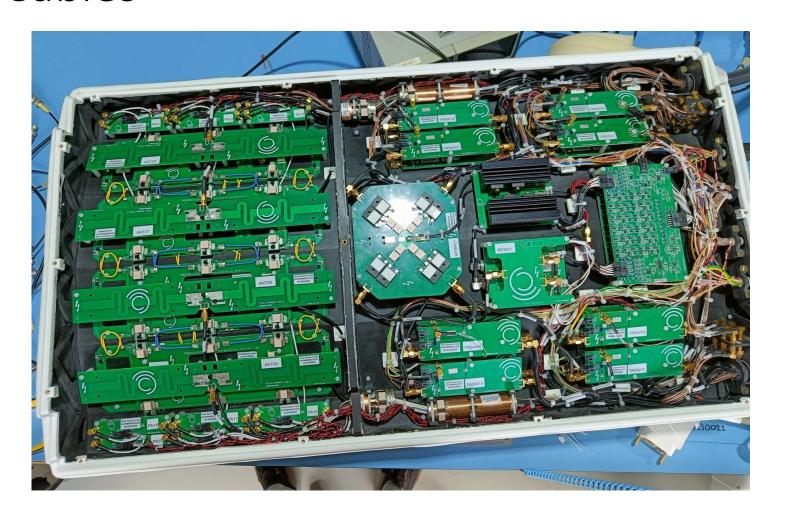






Sponsored by:

Cables









Summary

- Showed the electromagnetic field environment and application
- Component selection
 - Distortion of static magnetic field
 - SAR
 - High pulse power
 - Missing specifications
- Testing







Tesla Dynamic Coils

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